

Review Article

Molecular Imaging of Stem Cell Transplantation for Liver Diseases: Monitoring, Clinical Translation, and Theranostics

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Stem cell transplantation has been investigated to rescue experimental liver failure and is promising to offer an alternative therapy to liver transplantation for liver diseases treatment. Several clinical studies in this field have been carried out, but the therapeutic benefit of this treatment is still controversial. A major obstacle to developing stem cell therapies in clinic is being able to visualize the cells in vivo. Imaging modalities allow optimization of delivery, detecting cell survival and functionality by in vivo monitoring these transplanted graft cells. Moreover, theranostic imaging is a brand new field that utilizes nanometer-scale materials to glean diagnostic insight for simultaneous treatment, which is very promising to improve stem cell-based therapy for treatment of liver diseases. The aim of this review was to summarize the various imaging tools that have been explored with advanced molecular imaging probes. We also outline some recent progress of preclinical and clinical studies of liver stem cells transplantation. Finally, we discuss theranostic imaging for stem cells transplantation for liver dysfunction and future opportunities afforded by theranostic imaging.

1. Introduction

Acute liver failure and cirrhosis result from a variety of acute or chronic hepatic injuries [1, 2]. Up till now, liver transplantation has been considered as the primary treatment for acute liver failure and cirrhosis and various end-stage liver diseases. However, this procedure is hindered by the lack of donor organs, technical difficulties, complications associated with immune rejection, the requirement for lifelong immunosuppression, and financial considerations [3–5]. Therefore, to develop novel treatments that can either be effective curative and/or affect the underlying pathophysiology of the liver disease is urgently needed.

Stem cell transplantation has been suggested as an effective alternate approach for liver dysfunction [6–8]. For maximal efficacy, these therapies require transplanted cell delivery to targeted tissues followed by successful cell engraftment. So

far, numbers of clinic trials of stem cells transplantation for liver dysfunction have been carried out. By September 2016, more than 200 clinical trials had been registered when ClinicalTrials.gov was searched for the terms “stem cells AND liver diseases”. Among these clinical studies, some have indicated to be well tolerated and safe and confer beneficial effects in patients with liver failure, by enhancing liver function and reducing ascites and overall mortality without any major side effects [9–13]. However, the benefits of this emerging therapy for liver dysfunction in recent finished clinical trials are still conflicting. Some studies demonstrated there was no significant therapeutic effect to liver dysfunction [14]. Other concerns and critical issues remain unanswered regarding the long-term safety [9, 10, 12, 15–22]. Therefore, several meta-analyses have concluded that controversies remain in this rapidly developing field [23–26].

Meanwhile, several critical issues in clinical protocols require further investigation, such as the optimal type of cell types, the optimal therapeutic timing, the most effective stem cells amount, the best route of administration, and the primary endpoints. One thing is clear that there is an unmet clinical need to monitor the transplanted stem cells *in vivo*. Hence, *in vivo* visualization of transplanted stem cells with a robust, quantitative imaging method is essential for the monitoring of cell implantation, homing, and differentiation. The purpose of this current review is to summarize the latest developments of the various imaging modalities dedicated to monitor stem transplantation for liver dysfunctions; preclinical and clinic studies are emphasized; in addition, theranostic imaging and their future applications are also highlighted.

2. Imaging Methods to Monitor Transplanted Stem Cells in Animal Models

Noninvasive tracking of stem cells could facilitate its clinical translation. So far all major imaging modalities have been introduced to monitor transplanted stem cells for liver diseases. Numbers of animal studies have demonstrated that imaging modalities are essential for developing efficacious cell therapies for liver damage animal models.

2.1. Optical Imaging. Optical imaging, mainly based on retroviral vectors or enzymes to express fluorescent proteins, includes fluorescence imaging and bioluminescence imaging (BLI). Both these imaging methods have been tested for *in vivo* monitoring transplanted stem cells in liver.

Yukawa et al. investigated whether quantum dots (QDs) labeling using octa-arginine peptide (R8) for adipose tissue-derived stem cells (ASCs) could be applied for *in vivo* fluorescence imaging in mice with acute liver failure. The results demonstrated that heparin was effective in increasing the accumulation of transplanted ASCs in the liver using this imaging technology [27]. In another study, Akhan et al. conjugated a novel polymer based water-dispersible nanoparticles (CPN) with improved photostability, high fluorescent quantum yield, and noncytotoxicity compared to conventional dyes and quantum dots. The results showed that the labeled mesenchymal stem cells (MSCs) migrated to the liver and retained their labels in an *in vivo* liver regeneration model. These studies demonstrated that the utilization of fluorescence labeling could be a promising tool for the tracking of stem cells transplanted in liver to understand differentiation and homing mechanisms [28]. Wang et al. investigated upconversion nanoparticles- (UCNPs-) labeled mouse MSCs intravenous transplanted into mice and imaged using an *in vivo* upconversion luminescence (UCL) imaging system, observing the translocation of MSCs from lung where they initially accumulated, to liver [29]. Li et al. compared three-delivery routes for the MSCs transplantation to liver, including inferior vena cava (IVC), the superior mesenteric vein (SMV), and intrahepatic (IH) injection using *in vivo* BLI. Results showed that MSCs were firstly trapped inside the lungs, and no detectable homing to the liver and other organs was observed after IVC infusion; after SMV infusion,

MSCs were dispersedly distributed and stayed as long as 7-day posttransplantation in the liver. By IH injection, MSCs distribution was only localized in the injection region of the liver [30]. In another study reported by the same group, Liu et al. evaluated survival of transplanted human MSCs in the mice liver after intrahepatic transplantation and the role of intrahepatic natural killer (NK) cells by *in vivo* BLI. A gradual decline in bioluminescent signals from transplanted MSCs in liver was observed. Interestingly, compared to the control group, the survival time and retention of intrahepatic MSCs decreased more rapidly in the NK-activated group, which indicated that activated NK cells potentially accelerated the rejection of transplanted MSCs [31].

2.2. Nuclear Imaging. Wu et al. investigated the biodistribution of human placental deciduas basalis derived mesenchymal stem cells (PDB-MSCs) in nude mice after intravenous injection by carbon radioisotope labeling thymidine (^{14}C -TdR), which was able to incorporate into new DNA strands during cell replication. Labeled PDB-MSCs grafts were found mainly in the lung, liver, spleen, stomach, and left femur of the recipient animals at the whole observation period. This work demonstrated that ^{14}C -TdR labeling did not alter the biological characteristics of human placental MSCs and that this labeling method had potential to be used to quantify the transplanted cells in preclinical studies [32].

2.3. Magnetic Resonance Imaging (MRI). Magnetic resonance imaging provides high-resolution (ranging from $50\ \mu\text{m}$ in animals up to $300\ \mu\text{m}$ in whole body clinical scanners) images capable of tracking stem cells *in vivo* without invasiveness and without the use of ionizing radiation. Stem cells need to be prelabeled with contrast probes for cell tracking studies by MRI. The probes for MRI noninvasively identification and tracking of transplanted cells include negative contrast agents, as superparamagnetic iron-oxide (SPIO) and ultra-small superparamagnetic iron-oxide (USPIO) particles, and positive contrast agents, such as gadolinium. They both have been tested in small animal models for stem cells transplantation studies.

An emerging approach to visualizing stem cells by MR is to label the stem cells with perfluorocarbon (PFC) nanoemulsions, which can be detected with ^{19}F MRI.

2.3.1. SPIO. Bos et al. evaluated *in vivo* tracking of intravascularly injected SPIO labeled MSCs using a conventional 1.5 T MR imaging system. After labeled MSC injection, damaged liver had diffuse granular appearance. Cells were detected for up to 12 days in liver. They concluded that MRI could *in vivo* monitor intravascularly administered SPIO labeled MSCs in liver [33]. Arbab et al. developed a method of delivering SPIO labeled MSCs to a targeted area in an animal model by applying an external magnet. SPIO labeled MSCs were injected intravenously to animals, and an external magnet was placed over the liver area of the animals. MRI signal intensity (SI) changes in the liver were monitored at different time points using MRI. Interestingly, SI decrease in the liver after injection of MSCs was greater in rats with external

magnets and returned gradually to that of control rat livers at approximately day 29. The results proved that the external magnets retained the labeled MSCs in the region of interest [34]. Cai et al. evaluated *in vivo* MRI for tracking the SPIO labeled MSCs transplanted into rat liver through hepatic arterial infusion. The labeled stem cells in liver could be detected and monitored *in vivo* with a 1.5 T clinical MR scanner for up to 7 days after transplantation [35]. Ju et al. tracked intrasplenically transplanted MSCs labeled with SPIO by using MRI *in vivo* in a liver damaged rat model. These studies demonstrated that MSCs could be effectively labeled with approximately 100% efficiency. Migration of transplanted labeled cells to the liver was successfully documented with *in vivo* MRI [36, 37]. Choi et al. labeled human MSCs with SPIO and green fluorescence protein (GFP). Labeled MSCs were transplanted into the portal veins of immunosuppressed, hepatic-damaged rat models. Serial MR imaging showed signal loss in the liver of transplanted cells in the early period of transplantation [38]. Zhong et al. assessed SPIO labeled MSCs that were transplanted via the portal vein to rats with hepatic fibrosis using MRI. T2*-weighted MR imaging indicated lower signal in liver [39]. Kim et al. used a fluorescent magnetic nanoparticle (MNP), which had both magnetic and optical features, containing a ferritin core and a silica shell, and the inner portion of silica shell filled fluorescent materials for stem cell tracking studies. Intrasplenically transplanted MSCs labeled with MNP in liver cirrhosis rat model were monitored with 3T MR scanner. The results showed that the liver-to-muscle contrast-to-noise ratios at 3 and 5 h after cell transplantation was significantly lower than that of preinjection group [40].

2.3.2. Gadolinium Based Probes. Shuai et al. transfected human umbilical cord derived MSCs with gadolinium-diethylenetriaminepentaacetic acid (Gd-DTPA) for *in vitro* MRI. The result showed that minimum 5×10^4 Gd-DTPA-labeled stem cells could be detected with MRI *in vitro*. The trace duration time was about 12 days without compromising either cell viability or cell differentiability [41]. The same group also determined double labeling of MSCs with Gd-DTPA and fluorescent dye PKH26. Gd-DTPA and PKH26 were used to label the stem cells. MRI and fluorescence microscopy were used to detect the double-labeled MSCs. Their *in vitro* studies demonstrated that the proliferation and differentiation abilities of MSCs were not affected by double labeling using Gd-DTPA and PKH26 [42]. Furthermore, Pan et al. assessed tracking Gd-DTPA and PKH26-labeled human umbilical cord MSCs using MRI *in vivo*. The T1 values and signal intensity on T1-weighted imaging of labeled cells were significantly higher than the control. The signal intensity on T1-weighted imaging of labeled cells was retained over 14 days *in vivo* [43]. The results demonstrated that this labeling method was reliable and efficient; the *in vivo* studies of transplanted cells in liver using this labeling method need to be further investigated.

2.3.3. Perfluorocarbon Based MRI. Another technique under evaluation for imaging injected stem cells *in vitro* and *in*

vivo is based on perfluorocarbon (PFC) formulations, whose advantage is the high specificity due to the virtual absence of fluorine from the body. The fluorine signal can be accurately quantified from the MR images [44].

An emerging approach to imaging stem cells by MRI is to label the stem cells with perfluorocarbon nanoemulsions, which can be detected with ¹⁹F MRI [45–47]. The ¹⁹F nucleus is particularly suitable for labeling as its relative MR sensitivity is only 17% less than that of ¹H. Since the level of background ¹⁹F signal in host tissue is virtually absent [45], overlaying the ¹⁹F image on a conventional anatomical image allows for unambiguous, quantitative tracking of labeled cells *in vivo*.

A number of promising findings have been reported for the use of ¹⁹F labeling, including (1) intracellular labeling; (2) the lack of cellular toxicity; (3) the stability of cell labeling up to 21 days postlabeling; (4) positive signal with no background observed with ¹⁹F MRI; (5) biodistribution visualized by overlaying a ¹⁹F image of labeled cells on a ¹H anatomical image; (6) determination of the local concentration of labeled cells by quantitative ¹⁹F MRI [48].

2.4. Emerging Imaging Modality: Magnetic Particle Imaging (MPI). MPI is noninvasive and offers near-ideal image contrast, depth penetration, high sensitivity, and superb quantitative for single-cell tracking. Unlike MRI that applies magnetic resonance principles, MPI directly detects the iron-oxide nanoparticle-tagged cells using magnetic fields. These properties make MPI both ultrasensitive and linearly quantitative and very promising for monitoring transplanted cells *in vivo*. Conolly group from UC Berkeley firstly utilized MPI to monitor transplanted stem cells *in vivo* in animal model. Their first MPI cell tracking study demonstrated 200-cell detection limit *in vitro* and *in vivo* monitoring of graft clearance over 87 days in a rat model [49]. In a more recent study, this group imaged the intravenously transplanted MSCs using MPI. The results showed that labeled MSCs immediately entrapped in lung tissue posttransplantation and then relocated to the liver within one day. Longitudinal MPI-CT imaging demonstrated a clearance half-life of MSC iron-oxide labels in the liver at 4.6 days [50]. These first *in vivo* MPI results indicate that MPI offers strong utility for quantitating the transplanted stem cells labeled using SPIO.

3. Preclinic Imaging of Large Animal Models and Clinical Applications

Although stem cell transplantation based therapies have been clinically applied to patients, the fate of graft cells remains unknown. Small animal studies have demonstrated the feasibility and important role of *in vivo* imaging technologies for *in vivo* monitoring of transplanted stem cells. The next step is to conduct preclinic studies using large animals that are necessary for translation of these cutting edge imaging technologies to clinic.

3.1. Preclinic Imaging of Transplanted Stem Cells in Liver with Large Animal Models. Ito-Fujishiro et al. evaluated track

implanted peripheral blood mononuclear cells labeled with SPIO on days 0 and 7 after intravenous injection into a cynomolgus monkey using a 3T MRI scanner. Labeled cells were visualized in the liver on MR images T2-weighted sequences [51]. Shi et al. investigated tracking of SPIO labeled MSCs after intraportal transplantation to swine models of acute liver injury. Results showed that signal intensity loss in the livers of swine models by SPIO labeling on the T2*WI sequence persisted until 2 weeks after transplantation [52]. Spriet et al. compared the cell distribution and quantification shortly after intraportal vein, systemic intravenous and splenic injections of technetium-99m- (99mTc-) hexamethyl-propylene amine oxime (HMPAO) labeled MSCs in healthy beagle dogs. Scintigraphic images were obtained using gamma camera after cell transplantation to target the liver, which showed that, after the portal injection, diffuse homogeneous high uptake was observed through the liver; the systemic intravenous injection resulted in cells trapped in the lungs, whereas splenic injection led to MSCs mild splenic retention and homogeneous diffuse hepatic uptake [53].

3.2. The First Clinical Applications of Molecular Imaging on Stem Cells Transplantation for Liver Diseases. Gholam-rezanezhad et al. investigated the biodistribution of autologous ¹¹¹In-oxine labeled MSCs, after peripheral infusion in four cirrhotic patients was investigated using SPECT imaging. After intravenous infusion, the radioactivity was first observed to accumulate in the lungs of recipients. Then the radioactivity gradually increased in the liver and spleen in these four patients. Radiolabeled MSCs relocalized in liver and spleen: radioactivity decreased from 33.5% to 2% in lung and increased from 2% to 42% in spleen. This first clinic imaging study demonstrated that cell labeling with ¹¹¹In-oxine was a suitable tool for tracking peripheral vein infused MSC distribution [54]. In a more recent case report study, Defresne et al. assessed biodistribution of ¹¹¹Indium DTPA labeled adult derived human liver stem cells (ADLHSC) from healthy donor using SPECT imaging after infusion through the portal vein in a patient with glycogenosis type 1A. Following infusion through the portal vein, SPECT imaging observed ADLHSC spread strictly within the targeted organ of liver until 5 days [55].

4. Theranostic Imaging of Stem Cells

The term “theranostics” refers to a rapidly developing approach that combines diagnostic imaging and molecular therapy [56]. By packaging the two modalities of diagnostic imaging and molecular therapy together, the application of theranostic imaging is promising to overcome undesirable selective biodistribution differences between diagnostic imaging probes and therapeutic agents [57–60]. To achieve higher sensitivity and increase molecular specificity, the novel two-in-one theranostic agents for various imaging tools have been developed. Not only can the novel imaging probes be functional as imaging tools, but they can also be useful as a carrier for controlled releasing of therapeutic moieties [61].

4.1. Improving Liver Function by Delivering Therapeutic Plasmid DNA. Pang et al. utilized a complex of SPIO nanoparticle coated with polyethylene glycol-grafted polyethylenimine (PEG-g-PEI-SPION) as an MRI probe that can track of rat bone MSCs and also act as a carrier for the plasmid DNA. The complex labeled MSCs were modified by a plasmid encoding human hepatocyte growth factor (HGF) attached in the MRI visible vector complex and transplanted into fibrotic rat livers. The results proved that these transplanted grafts effectively restored albumin production and significantly suppressed transaminase activities in the liver damaged animal models. Meanwhile, the transplanted MSCs displayed a sensitive signal on T2/T2*-weighted MR images, which enabled in vivo tracking of the cells for up to 14 days after transplantation [62].

4.2. Promoting Transplanted Cell Survival by Combined Cytokines Delivery. Kempen et al. designed a theranostic mesoporous silica nanoparticle that could offer ultrasound and MRI signal to guide transplanted cells and also served as a drug release reservoir of insulin-like growth factor (IGF) that could promote MSCs survival. The results showed that the presence of IGF increased cell survival up to 40% versus unlabeled cells in vitro [63]. Pulavendran et al. compared cirrhotic mice received either hematopoietic stem cells (HSC) or MSC with or without HGF incorporated chitosan nanoparticles (HGF-CNP). Serum levels of selected liver protein and enzymes were significantly increased in the combination of MSC and HGF-CNP (MSC+HGF-CNP) treated group. These findings indicated that HGF-CNP enhanced the differentiation of stem cells into hepatocytes. The results demonstrated MSCs transplantation in combination with HGF-CNP could be a promising treatment for liver cirrhosis [64].

4.3. In Vivo RNA Interference: siRNAs and microRNAs Delivery Carriers. RNA interference is a naturally occurring endogenous regulatory process where short double-stranded RNA including small interference RNA (siRNA) and microRNAs could induce sequence-specific posttranscriptional gene silencing. In vivo RNA interference therapy represents a promising therapeutic strategy, but the barriers for delivery siRNAs or microRNAs hamper this therapeutic method to reach their intended targets cells or tissues and to exert their gene silencing activity [65]. Theranostic probes labeled on the transplanted stem cells actually could serve as siRNA or microRNA carriers. Zhao et al. synthesized poly-sodium4-styrenesulfonate (PSS) and poly-allylamine hydrochloride (PAH) coated AuNR-based nanoparticles, which could deliver siRNA against LSD1 to induce the hepatocyte lineage differentiation of human MSCs in vitro [66]. These methods need to be further tested in vivo before it could eventually translate to clinical applications. MicroRNAs are endogenous small noncoding RNAs that regulate key processes of cells. Studies have been reported on the posttranscriptional regulation of hepatic differentiation and regenerative capacities in MSCs by microRNAs [67, 68]. Gomes et al. reported the use of biodegradable nanoparticles

containing perfluoro-1,5-crown ether (PFCE), a fluorine-based compound (NPI70-PFCE) that could track cells in vivo by MRI and efficiently release miRNA. NPI70-PFCE conjugated with miRNA132 could accumulate within the cell's endolysosomal compartment increased 3-fold the survival of endothelial cells (ECs) transplanted in vivo [69]. This novel theranostic technology potentially could be transferred to stem cells transplantation for liver diseases in future.

4.4. Stem Cells Can Be Used as a Unique Carrier for Therapeutic Agents. Zhao et al. loaded adipose-derived MSCs with SPIO-coated gold nanoparticles (SPIO@AuNPs), which is a MR contrast probe that can be activated to generate heat when irradiated with near-infrared laser, and tested their effects against liver injury and hepatocellular carcinoma (HCC) in mice. The results showed that in vivo MR imaging confirmed the active homing of AD-MSCs to liver. Upon laser irradiation, the SPIO@AuNP-loaded AD-MSCs could thermally ablate surrounding HCC tumor cells.

This study demonstrated that AD-MSC could act as an efficient carrier for therapeutic agents to liver injuries or HCC. The results showed that SPIO@AuNP-loaded AD-MSCs proved a promising theranostic agent for liver injury and HCC [70].

4.5. Preventing Teratoma Formation in Target Organs. One reason for controversial application of stem cell treatment is the possibility associated with tumor formation in the recipient. For promoting therapeutic effect, stem cells may undergo substantial manipulation such as differentiation and in vitro expansion, and this can lead to possible genetic aberrations and carcinogenesis [71]. To address the intractable issues such as the teratoma formation encountered in human embryonic stem cell (hESC) for therapeutic in clinic, Chung et al. hypothesized that serial manganese-enhanced MRI would have theranostic effect to assess hESC survival, teratoma formation, and hESC-derived teratoma reduction through intracellular accumulation of Mn²⁺. The study demonstrated that systemic administration of MnCl₂ enabled simultaneous monitoring and elimination of hESC-derived teratoma cells by higher intracellular accumulation of Mn²⁺ [72].

5. Conclusions and Future Perspectives

Stem cell therapy as a part of regenerative medicine provides promising alternatives for the treatment of liver injuries and diseases. The increasing application of stem cells transplantation for liver diseases treatments created the demand for long-term and quantitative in vivo cell tracking methods [71]. In this review, promising in vivo imaging methods for stem cell monitoring after transplantation in liver are shown. It is unlikely that one technique will answer all questions, but use of a multimodal approach will be the most appropriate approach to addressing the number of issues posed in this exciting field. The selection of a set or a combination of appropriate imaging approaches will depend on the goal of the experiment, on the experimental subject under study, and also on the availability of multimodality imaging facilities

and probes. In addition, new imaging modalities including Cherenkov illumination imaging (CLI), photoacoustic imaging (PAI), and surface enhanced Raman imaging (SERI) are developing rapidly. The application of these new strategies will also play a helpful role in the advancement of the field of stem cell therapy [73]. Mostly, although still in its infant stage of development, theranostic imaging definitely represents a promising new direction for in vivo stem cell transplantation. The maturation of multifunctional theranostic imaging may indeed revolutionize stem cell transplantation approach for liver diseases and beyond [74].

Competing Interests

The authors declare that there are no competing interests regarding the publication of this paper.

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